

Medical Staff Dosimetry

Summary of the Submitted Problem Solutions

Medical Staff Dosimetry

Restricted Problem – CONRAD WP4 & WP7

Jean-Marc Bordy - Design of a Realistic Calibration
Field for Diagnostic Radiology

Frank Schultz - Simulation of an Interventional
Cardiac Catheterization
Procedure

Lara Struelens - Summary of the Submitted
Problem Solutions

Outline

Problem 1:

A comparison of calculated results and experimental data concerning the characterization of the scattered field

- Belgium (MCNPX)
- The Netherlands (MCNP4C)
- Slovakia (MCNP4C)
- Portugal (MCNPX)
- Denmark (Penelope 2006)

Problem 2:

A comparison of calculated results concerning the dose to the interventional cardiologist

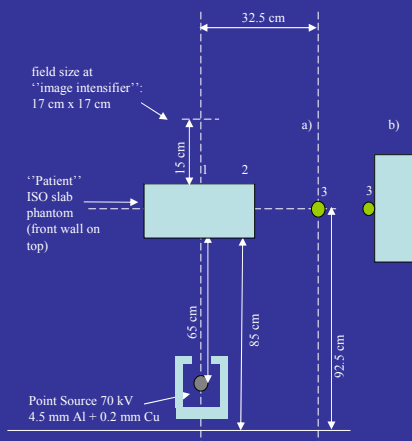
- Belgium (MCNPX)
- The Netherlands (MCNP4C)
- Portugal (MCNPX)
- Denmark (Penelope 2006)



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Problem 1: A comparison of calculated results and experimental data concerning the characterization of the scattered field



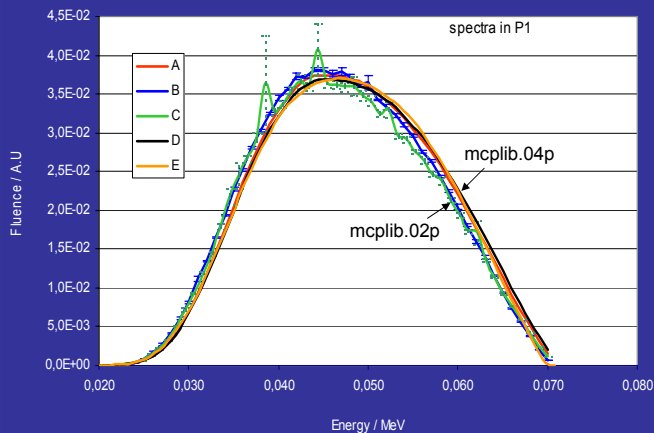
- Calculate energy spectra at P1 and P2
- Calculate 'dosimeter' readings (P3) per unit of dose-area-product (DAP)
 - a. Free-in-air
 - b. In front of 'cardiologist' phantom
- Comparison with experiments: intercomparison of APDs at CEA and IRSN (CONRAD-WP7)



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Results: Energy spectra at P1



Average energy:

- A: 47.97 keV \pm 0.06%
- B: 47.26 keV \pm 0.25%
- C: 47.26 keV \pm 1.08%
- D: 48.23 keV \pm 0.04%
- E: 47.96 keV \pm 0.18%

Standard deviation: 0.90%

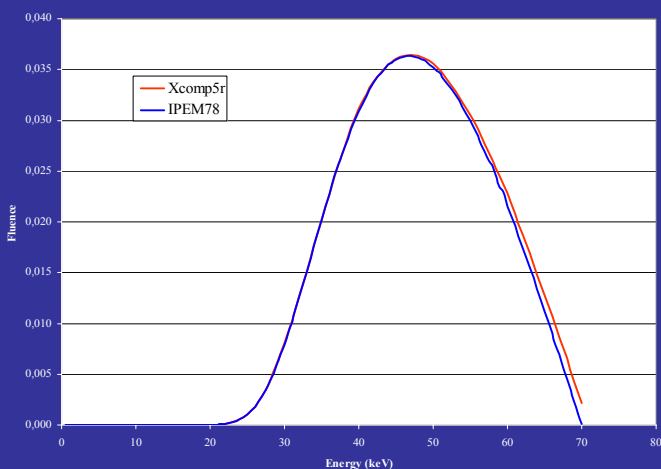
- Cross section libraries
- Source spectrum: Xcomp5r \leftrightarrow IPEM78



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source spectrum generator



- A: Xcomp5r
- B: IPEM78
- C: Xcomp5r
- D: Xcomp5r
- E: Xcomp5r

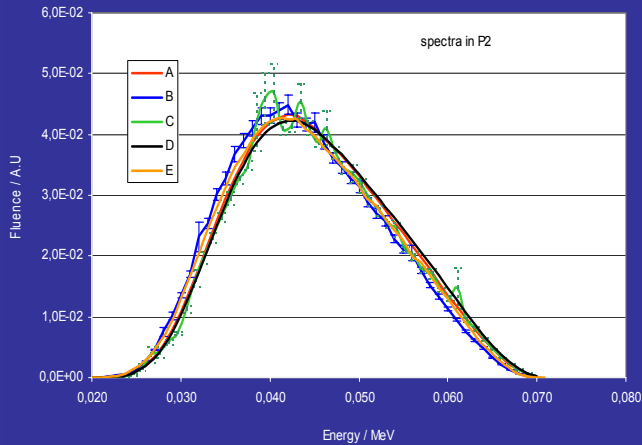
Source spectrum: Xcomp5r \leftrightarrow IPEM78



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Results: Energy spectra at P2



Average energy:

- A: 45.10 keV \pm 0.07%
- B: 44.10 keV \pm 0.55%
- C: 45.15 keV \pm 1.50%
- D: 45.40 keV \pm 0.07%
- E: 44.53 keV \pm 0.51%

Standard deviation: 1.18%

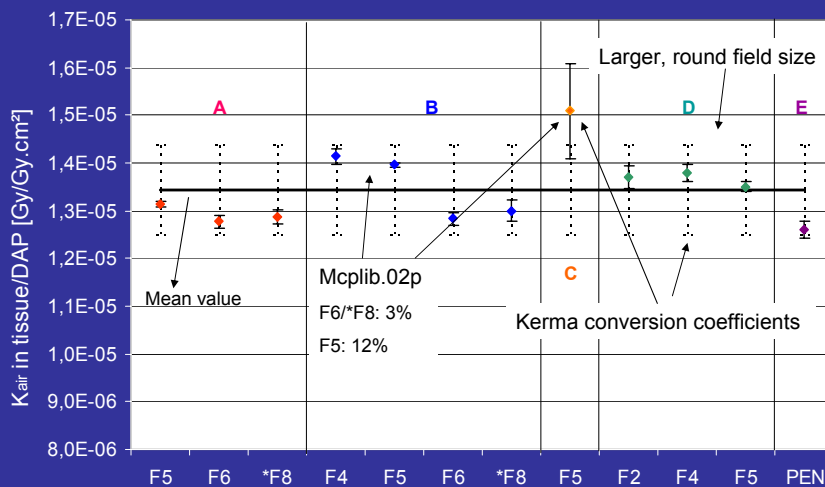
- Cross section libraries
- Source spectrum: Xcomp5r \leftrightarrow IPEM78



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Results: 'Dosimeter readings' free-in-air

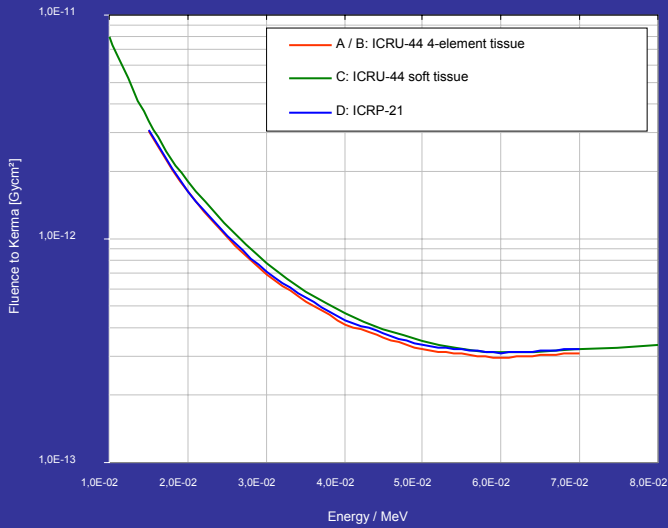


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conversion coefficients

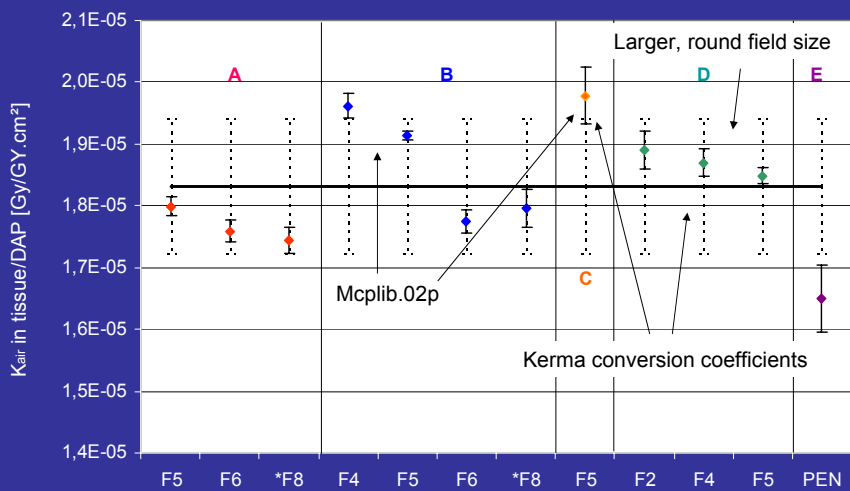
$$K = \int \overline{\Phi}_E \cdot E \cdot \left(\frac{\mu_{tr}}{\rho} \right) \cdot dE$$



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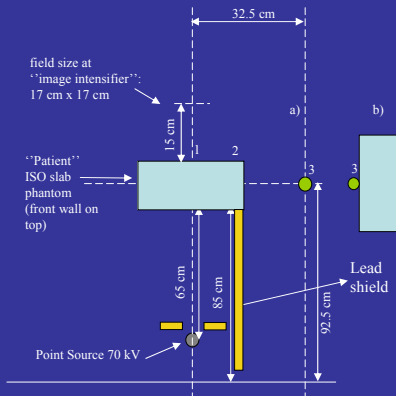
Results: 'Dosimeter readings' in front of slab phantom



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Comparison with experiments



APD intercomparison with same ISO slab geometry.

CEA: pulsed radiation
square field

IRSN: continuous radiation
round field



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Comparison with experiments

Measurements:

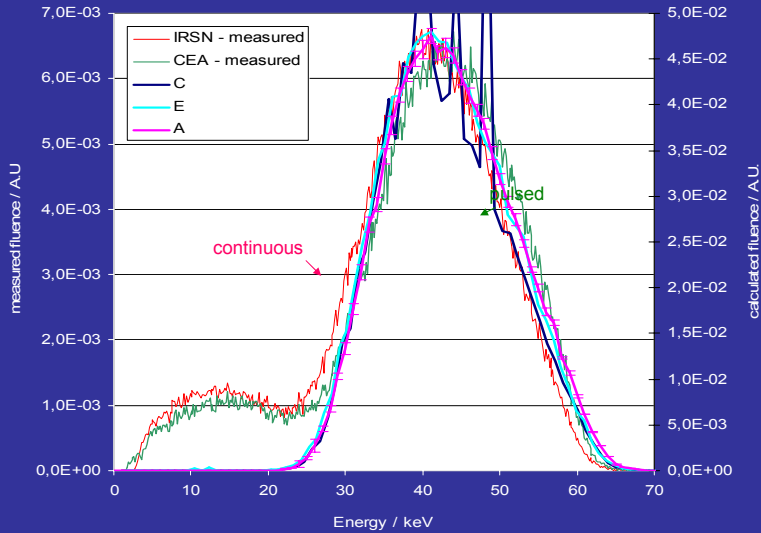
- Energy spectra in point 3 free-in-air (CdTe XR-100T spectrometer)
→ compared to calculated spectra in point 3 (A, C and E)
- Air kerma K_{air} at point 3 free-in-air (ionisation chamber)
→ compared to calculated values in point 3 (A, B, C, D and E)



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Comparison with experiments



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Comparison with experiments

Measurements:

- Energy spectra in point 3 free-in-air (CdTe XR-100T spectrometer)
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Comparison with experiments

- Air kerma K_{air} at point 3 free-in-air
- Measurements with ionisation chamber
 - Pulsed: $15.7 \mu\text{Gy}/\text{Gycm}^2$ ($k = 2$; uncertainty: 6.2%)
 - Continuous: $10.2 \mu\text{Gy}/\text{Gy.cm}^2$ ($k = 2$; uncertainty: 7.3%)
- Calculations **Only results using mcplib.04p**
 - Kerma in tissue $\rightarrow K_{\text{air}} : (\mu_{\text{en}}/\rho)_{\text{air}} / (\mu_{\text{en}}/\rho)_{\text{tissue}}$
(ICRU-44 ; the complete spectra from institutes was taken into account)
 - Average $K_{\text{air}} = 12.3 \mu\text{Gy}/\text{Gy.cm}^2$ (uncertainty: 1.5 %)
- Systematic error: 22% (pulsed) and -20% (continuous)



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Conclusions problem 1

- Problems were solved using different codes: MCNP4C, MCNPX and Penelope
- The main differences between the calculated results were the choice of library and the choice of dose conversion coefficients
 - \rightarrow flux tallies are sensitive to angular distributions of secondary particles
 \Rightarrow recommended to use the latest set of data tables: mcplib.04p
 - \rightarrow differences were larger than the statistical uncertainties
- Systematic error of $\pm 20\%$ between experimental and calculated data
 - \rightarrow Where do the differences in experimental data come from?
 - \rightarrow calculations done in a sphere filled with tissue \leftrightarrow air kerma measurement
 - \rightarrow Simulation of environment necessary?

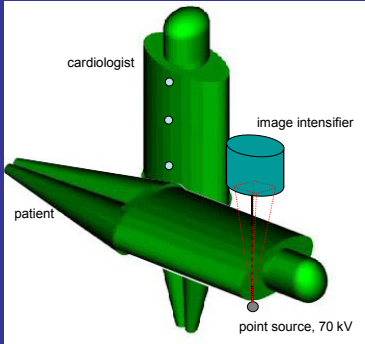


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Problem 2: A comparison of calculated results concerning the dose to the interventional cardiologist

A representative clinical practice



- Calculate 'dosemeter readings' per DAP at waist, chest and neck level
 - a. Without protective clothing
 - b. Above and under lead-apron
- Calculate effective dose to the cardiologist per DAP
 - a. Without protective clothing
 - b. With protective clothing

Geometry, technical parameters: pres. F. Schultz



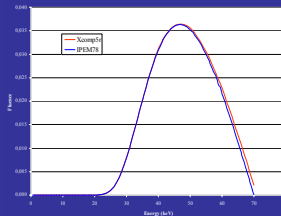
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Problem 2: A comparison of calculated results concerning the dose to the interventional cardiologist

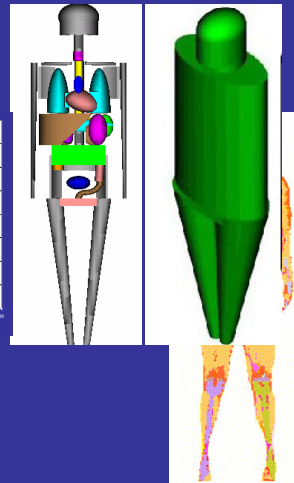
Implementation of clinical situation by participant:

- choice of spectrum generator
 - A, D and E: X-comp5r
 - B: IPEM78



- choice of phantoms

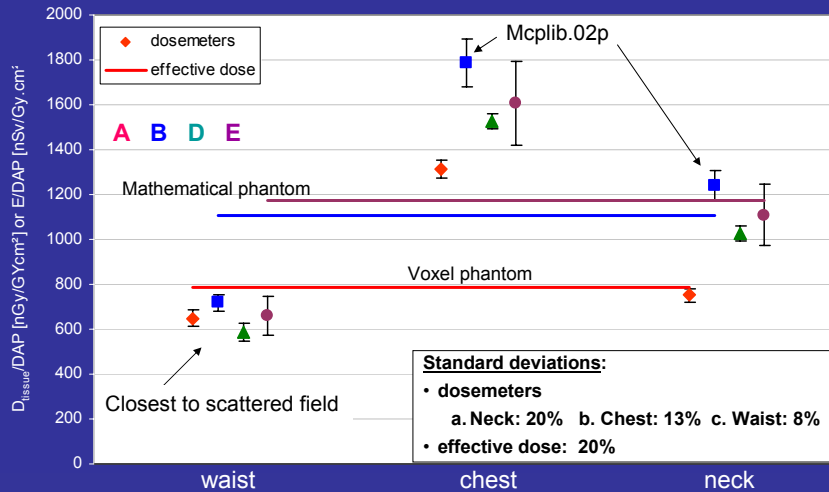
- Patient: mathematical phantom (ADAM, Bodybuilder)
- Staff: B, D and E: ADAM mathematical phantom
- A: MAX voxel phantom



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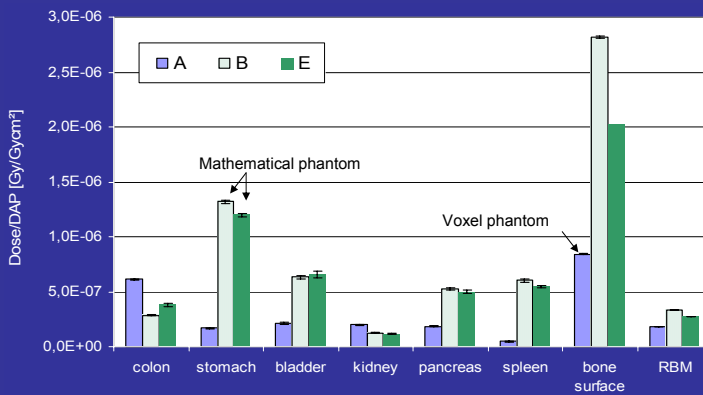
Results: without protective clothing (4 participants)



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Results: without protective clothing: organ doses



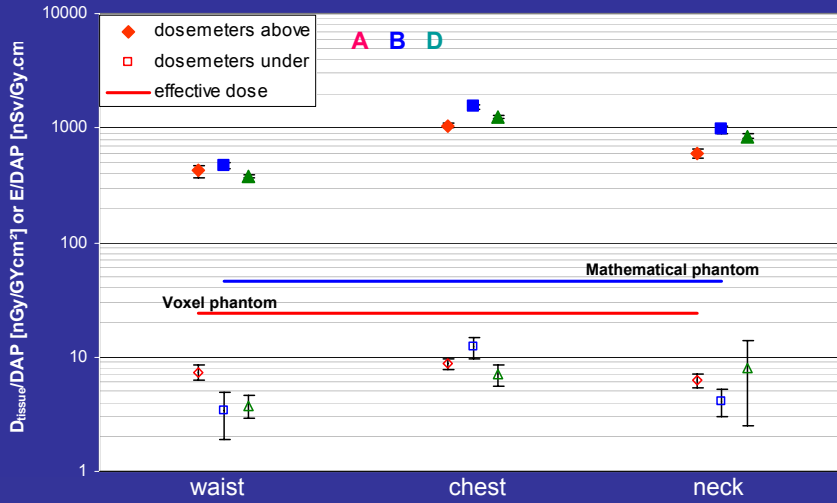
- Different phantoms
- Calculation method for skeleton and Red Bone Marrow (RBM): skeleton mixture, distribution of RBM, correction factors, ...



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Results: with protective clothing (3 participants)



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Results: with protective clothing

differences:

- dosemeters above
 - Neck: 24%
 - Chest: 19%
 - Waist: 11%
- dosemeters under
 - Neck: 32%
 - Chest: 28%
 - Waist: 45%
- effective dose: 47% (only 2 results)

Ratio $H_p(10) / E$:

- dosemeters **above** apron: **average overestimation of E by a factor of 25**
 minimum: factor 10 (waist dosimeter)
 maximum: factor 43 (chest dosimeter)
- dosemeters **under** apron: **average underestimation of E by a factor 0.22**
 minimum: factor 0.35 (chest dosimeter)
 maximum: factor 0.07 (waist dosimeter)

⇒ Need of algorithm to combine 2 dosimeters for conservative estimation of E



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Results: with protective clothing

Example of 2 existing algorithms

1. From a large Belgian study: $E_{\text{est}} = 2.25 \times H_p(10)_{\text{thorax, under}} + 0.097 \times H_p(10)_{\text{neck, above}}$

Results for A: $E_{\text{est}} = 77 \text{ nSv/Gy.cm}^2$ and $E_{\text{calc}} = 24 \text{ nSv/Gy.cm}^2$
ratio $E_{\text{est}} / E_{\text{calc}} = 3.16$ (overestimation of 216%)

Results for B: $E_{\text{est}} = 122 \text{ nSv/Gy.cm}^2$ and $E_{\text{calc}} = 45 \text{ nSv/Gy.cm}^2$
ratio $E_{\text{est}} / E_{\text{calc}} = 2.69$ (overestimation of 169%)

2. From Wambersie: $E_{\text{est}} = 1.0 \times H_p(10)_{\text{waist, under}} + 0.1 \times H_p(10)_{\text{neck, above}}$

Results for A: $E_{\text{est}} = 67 \text{ nSv/Gy.cm}^2$ and $E_{\text{calc}} = 24 \text{ nSv/Gy.cm}^2$
ratio $E_{\text{est}} / E_{\text{calc}} = 2.74$ (overestimation of 174%)

Results for B: $E_{\text{est}} = 101 \text{ nSv/Gy.cm}^2$ and $E_{\text{calc}} = 45 \text{ nSv/Gy.cm}^2$
ratio $E_{\text{est}} / E_{\text{calc}} = 2.22$ (overestimation of 122%)

NOTE: result for only 1 configuration (PA thorax), 1 spectrum, 1 position of cardiologist!!!



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Conclusions problem 2

Monte Carlo modelling for medical staff dosimetry – difficulties

- A realistic clinical situation is a combination of a very large amount of parameters
 - Beam projections (PA, AP, LAT, OBL, ...)
 - Field sizes ($17 \times 17 \text{ cm}^2$)
 - Irradiated parts of the patient (head, thorax, abdomen, ...)
 - Energy spectra: combination of tube voltage and filtration (60, 70 - 100 kVp; 2.0-4.0 mm Al + 0.1, 0.2-0.6 mm Cu)
 - Position of the worker in respect to the scattered radiation field
- There is **a large influence** on how a clinical practice is implemented in a calculation problem for the evaluation of the effective dose to the worker
 - Larger difference in effective dose than in dosimeter results between participants
 - ⇒ Different correlation between dosimeters results and effective dose
 - ⇒ Different results between participants when 1 specific algorithm is used



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Conclusions problem 2

- Minimise this influence by
 - type of phantom, organ dose calculation
 - 1 reference phantom (voxelised) for dose and radiation protection studies
 - data libraries, statistical uncertainties
 - most recent libraries
 - under lead apron: variance reduction techniques
- There will always remain a large systematic uncertainty between calculation results and reality due to the difference in anatomy between real persons and a reference phantom



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Uncertainty Assessment in Computational Dosimetry:

A comparison of Approaches



Thanks to all participants !!!



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