

Dosemeter Algorithms

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Two element whole body dosemeter



- **HARSHAW** dosemeter card
- **2 LiF:Mg,Ti chips**
(3.2 mm x 3.2 mm x 0.38 mm) .
- The wrapped card is worn in a service specific dosemeter badge (containing the different filter elements)
- Application of a **dose algorithm** on the basis of the dose information of each single TL chip allows the calculation of the personal dose in the appropriate dose quantity.

*Example for application
of Algorithms*



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Radiation Measurements 43 (2008) 571–575

Radiation Measurements

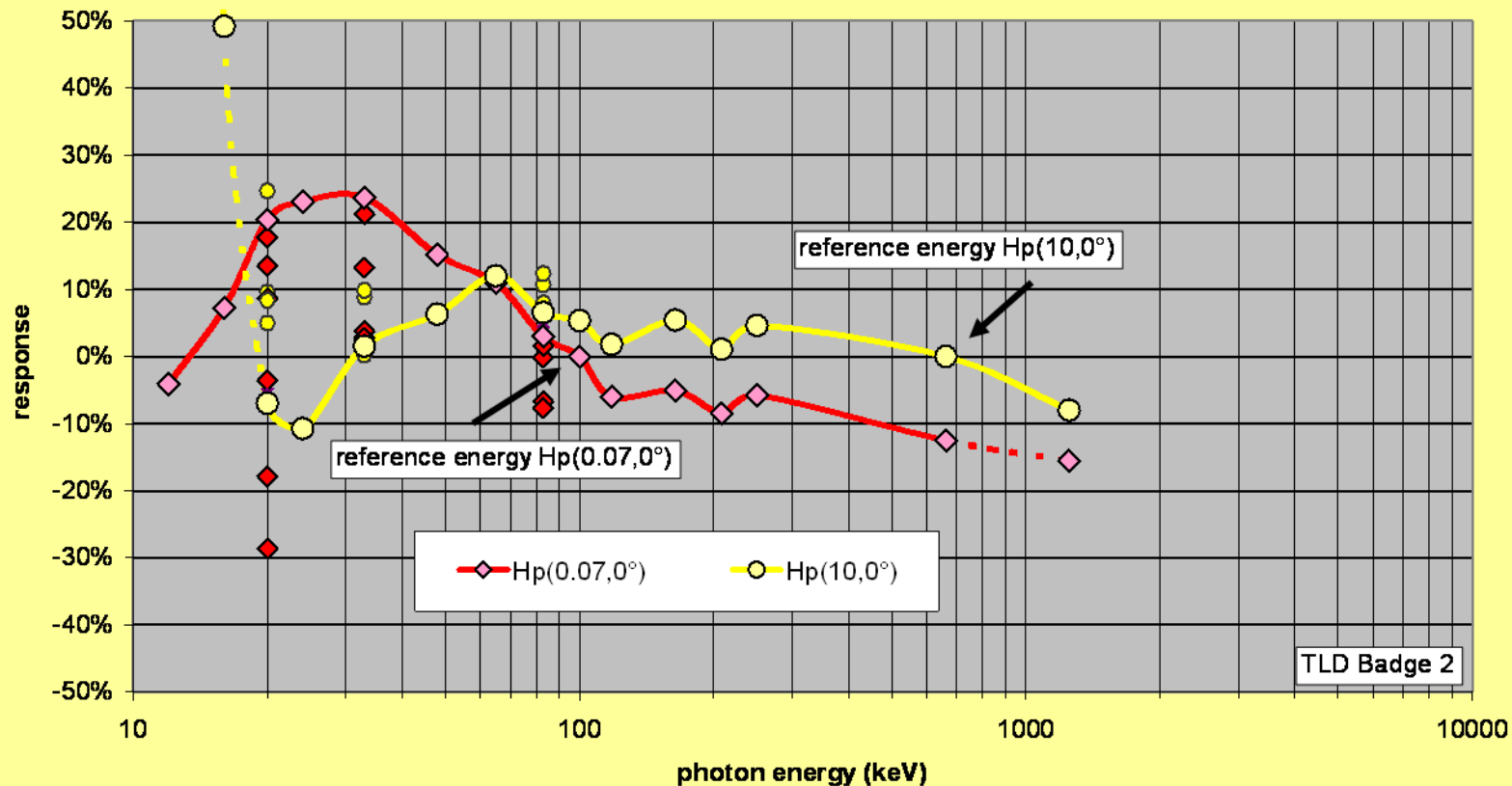
www.elsevier.com/locate/radmeas

Comparison of different dose algorithms used to evaluate a two element LiF:Mg,Ti TL personal dosimeter

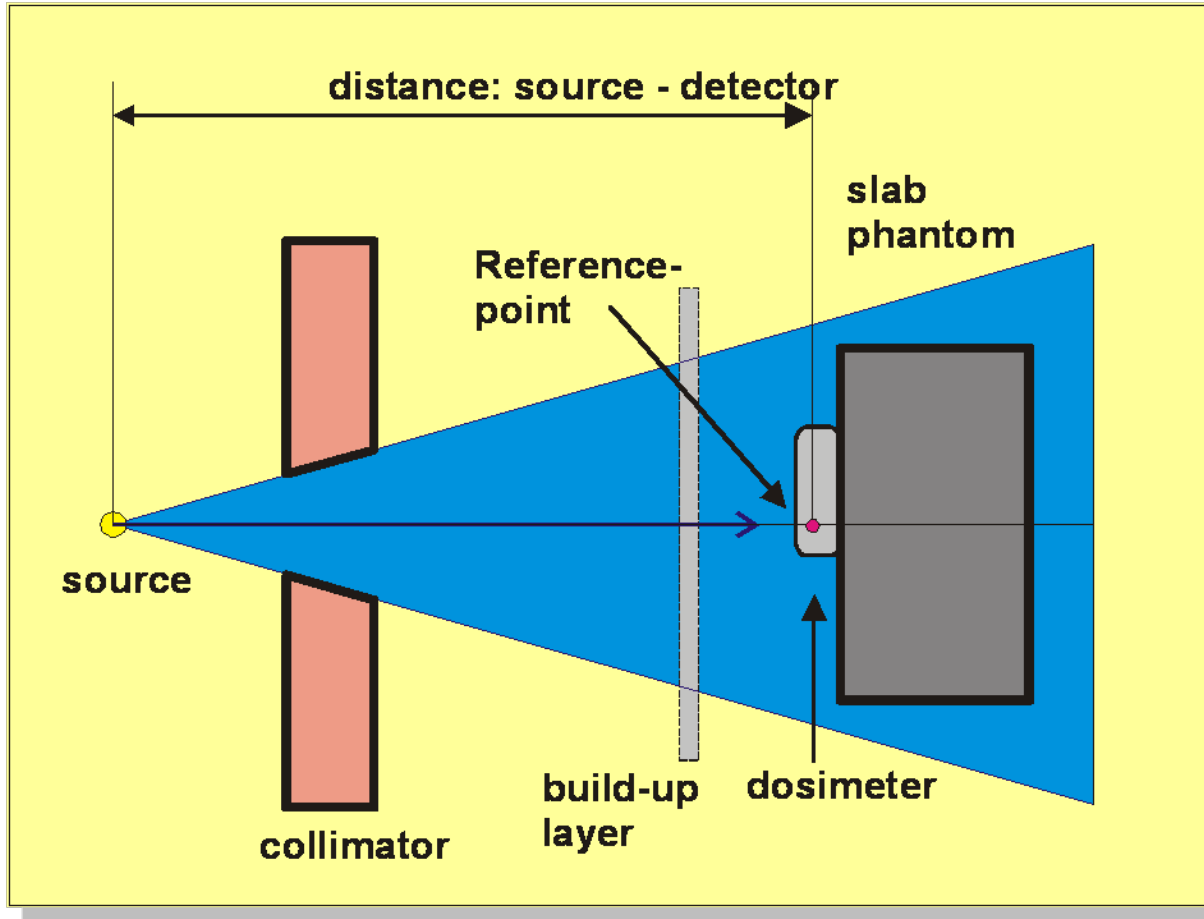
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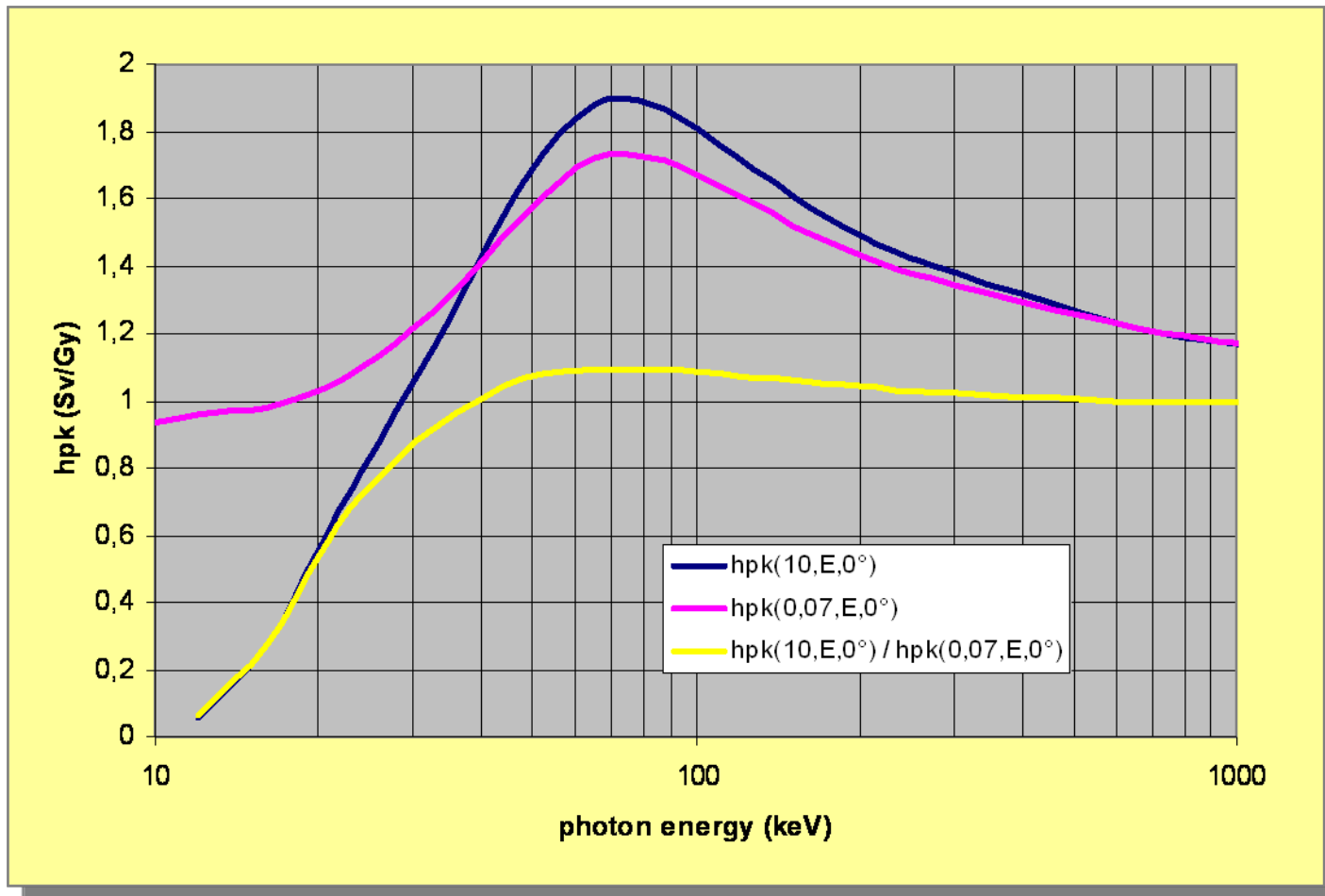
Energy and directional response for whole body dosemeter for $H_p(10)$ and $H_p(0,07)$



Calibration on the phantom (H_p)



Conversion factors h_{pk} (ISO 4037-1)



Dose Quantity used in Austria for personal monitoring

- Photon dose equivalent H_x [Sv]
 - Definition: $H_x = 0.01 \text{ Sv/R} \cdot X$
 - Relation: $H_x \cong 1.139 \text{ Sv/Gy} \cdot K_a$
X standard exposure
 K_a air kerma
- Personal dose equivalent $H_p(d)$ [Sv]
 - $H_p(10)$
 - $H_p(0.07)$

The **kerma**, K , is the quotient of dE_{tr} by dm , where dE_{tr} is the sum of the initial kinetic energies of all the charged particles liberated by uncharged particles in a mass dm of material, thus

$$K = \frac{dE_{tr}}{dm}.$$

Unit: J kg^{-1}

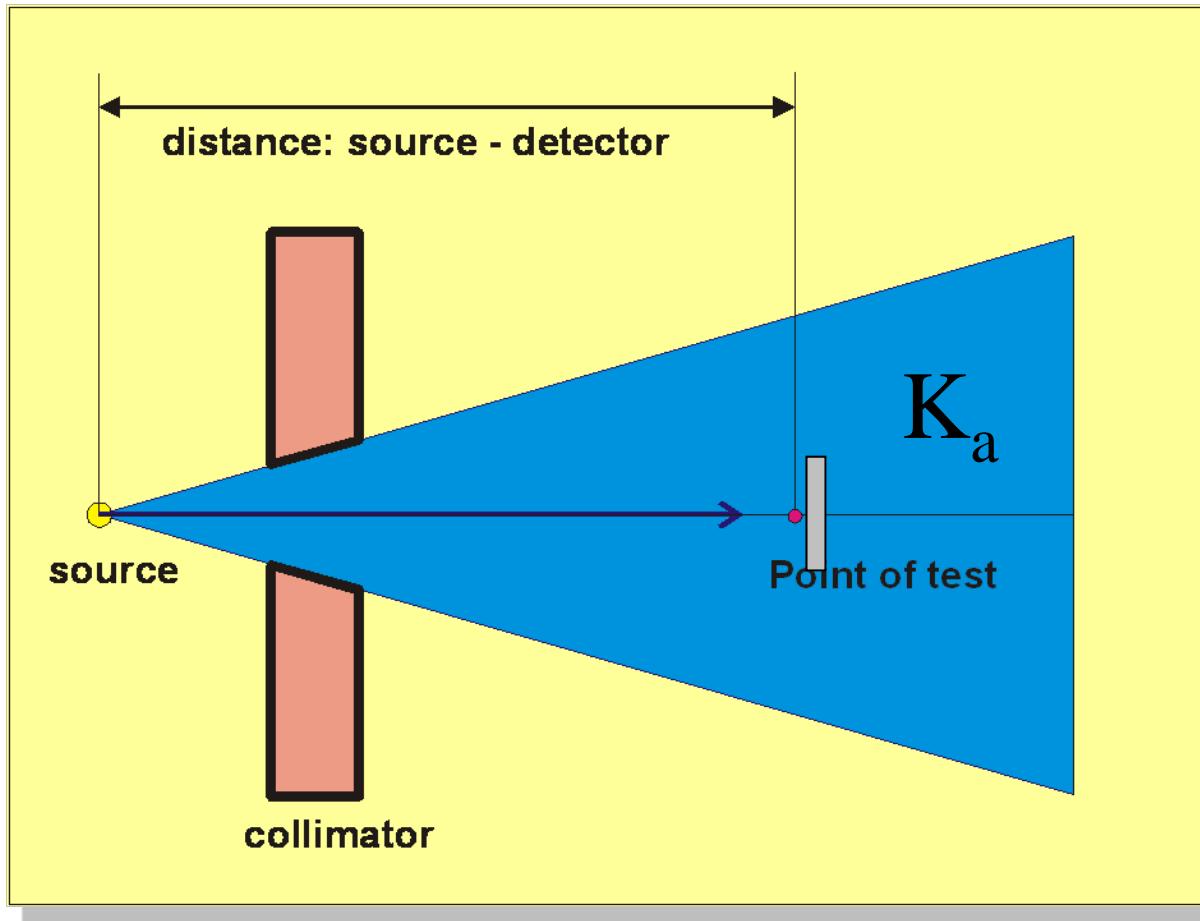
The special name for the unit of kerma is gray (Gy).

The personal dose equivalent, $H_p(d)$, is the dose equivalent in soft tissue, at an appropriate depth, d , below a specified point on the body.

Unit: J kg^{-1}

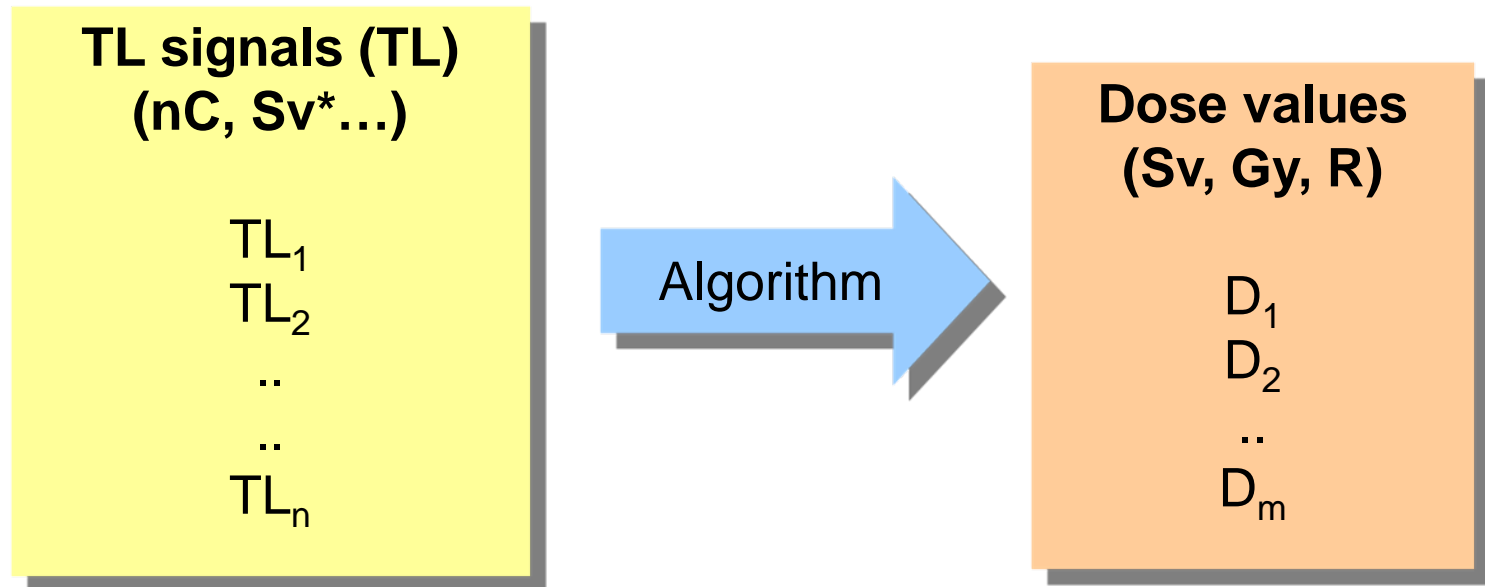
The special name for the unit of personal dose equivalent is sievert (Sv).

Free in air calibration (K_a)

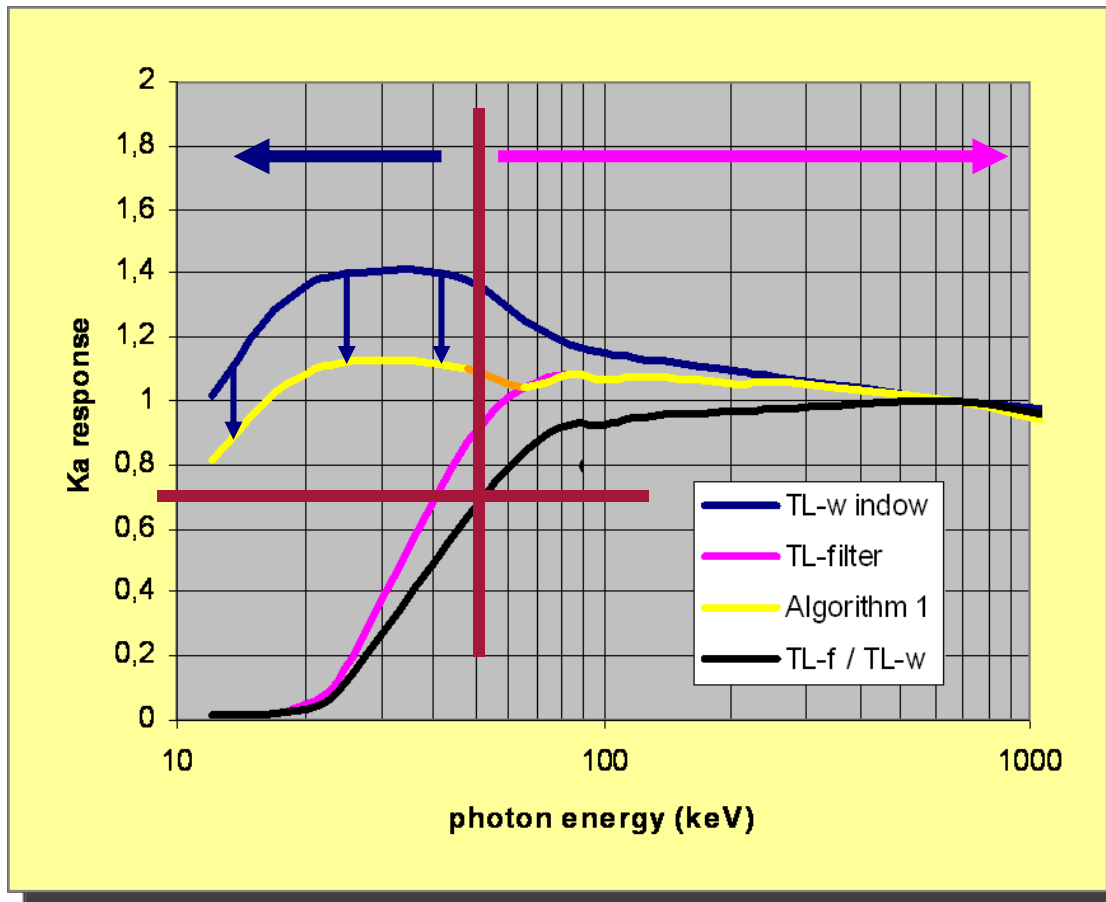


Dose Algorithm

- Each of n TL-Element gives (at least) one detector signal TL_i
- **Combination of all detector signals** TL gives dose values D_i in the appropriate dose quantity



Algorithm 1 (for Air Kerma / free in air)



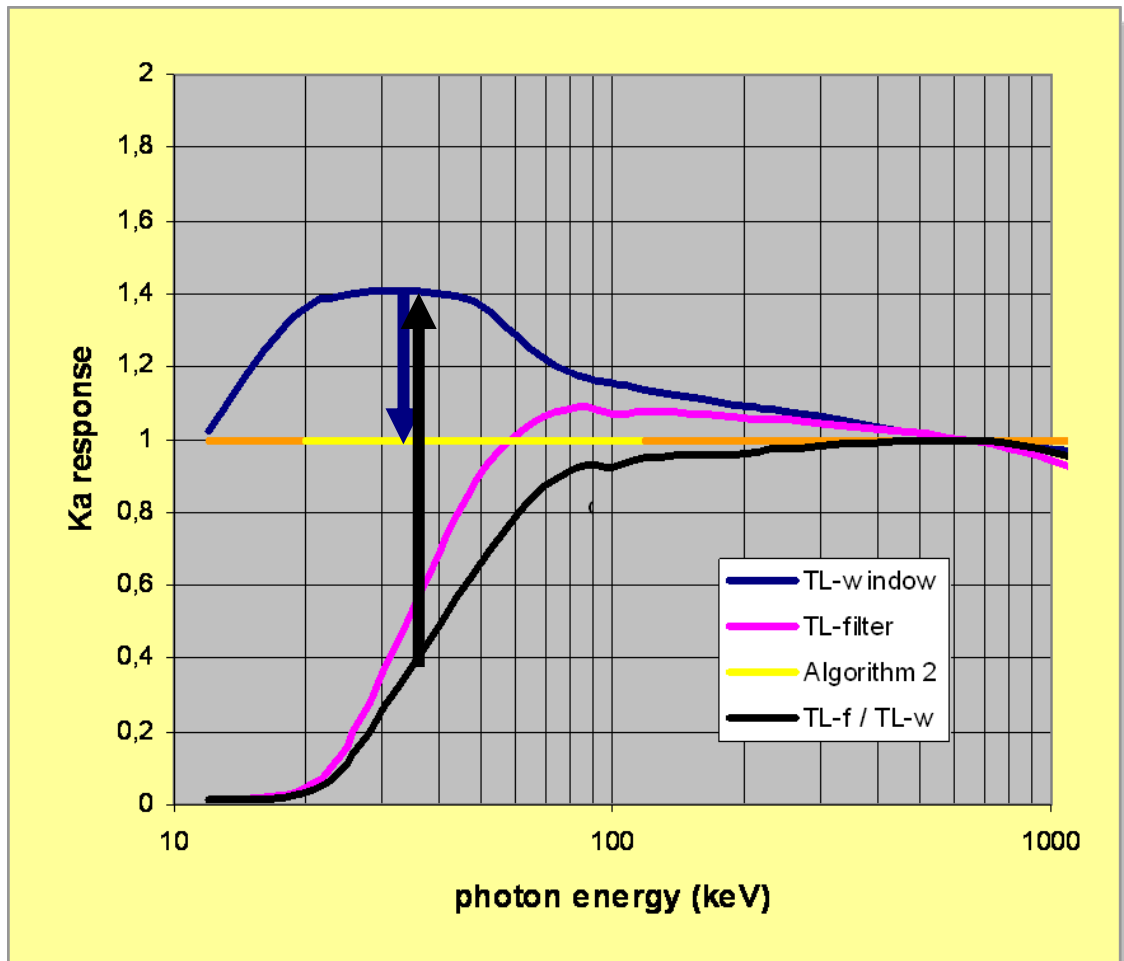
"if" dose algorithm 1:

$$\frac{TL_f}{TL_w} \geq 0.7 \Rightarrow K_a = N \cdot TL_f$$

$$\frac{TL_f}{TL_w} < 0.7 \Rightarrow K_a = N \cdot 0.8 \cdot TL_w$$

\Rightarrow energy response $< \pm 20\%$

Algorithm 2 (for Air Kerma / free in air)



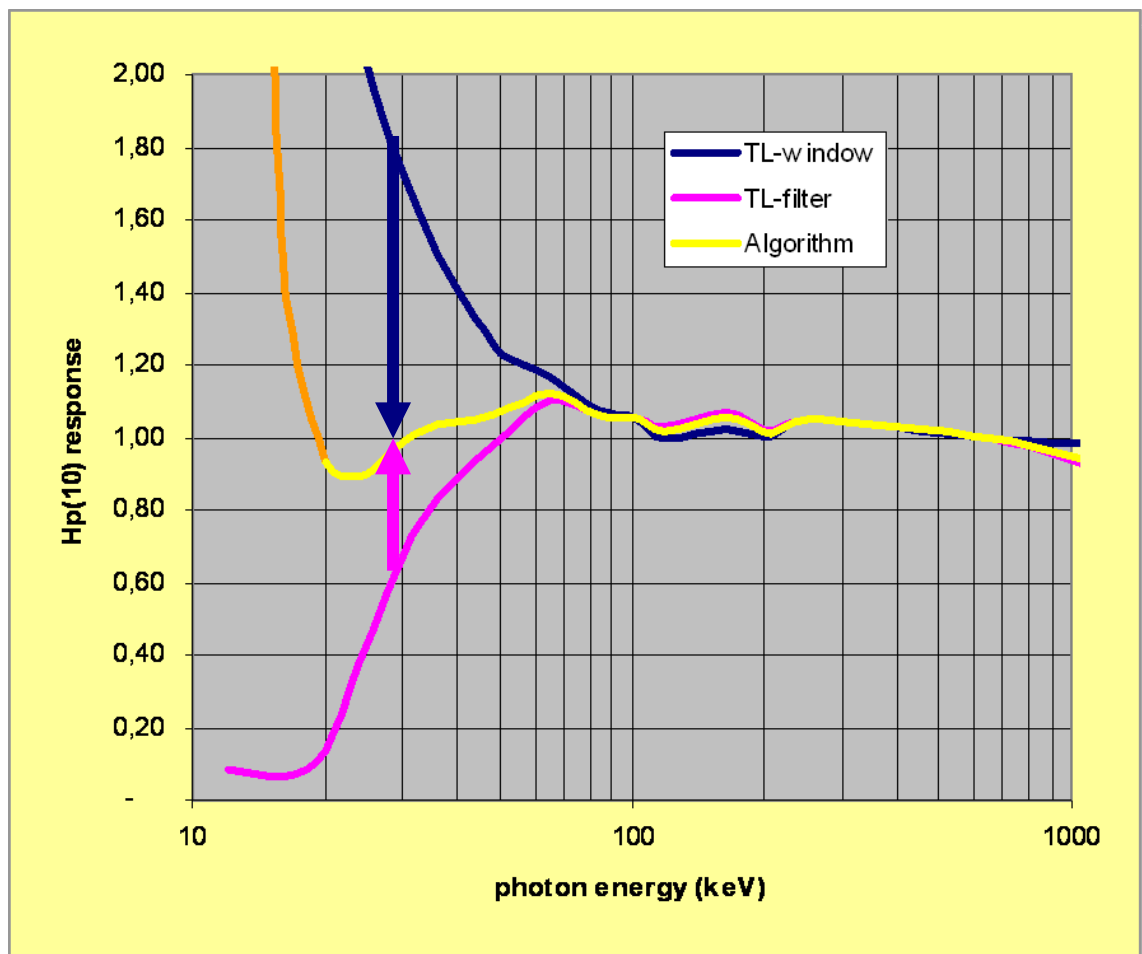
"special" dose algorithm 2 :

$$K_a = N \cdot \frac{TLW}{f_w \left(\frac{TLf}{TLW} \right)}$$

$f_w(R)$energy respons of TLW

⇒ Energy response ≈ 0%

Algorithm 3a (for $H_p(10)$ / on slab phantom)



"linear" dose algorithm 3a :

$$H_p(10) = N \cdot (a \cdot TL_w + (1 - a) \cdot TL_f)$$

⇒ Energy response < ±15%

⇒ Reference radiation quality : S - Cs

Dose algorithms used in Europe

Radiation Protection Dosimetry (2004), Vol. 112, No. 1, pp. 45–68
doi: 10.1093/rpd/nch283

A CATALOGUE OF DOSEMETERS AND DOSIMETRIC SERVICES WITHIN EUROPE—AN UPDATE

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- **From 43 European services:**
 - No algorithm: 60%
 - „If“ algorithm: 10%
 - Linear combination: 30%

Linearity of Algorithms

Linearity :

$D(\dots) \dots H_x, H_p(10), H_p(0.07)$

$$\underline{D(TLw_1 + TLw_2, TLf_1 + TLf_2)} = \underline{D(TLw_1, TLf_1)} + \underline{D(TLw_2, TLf_2)}$$



Algorithms

Linearity :

$$D() \dots\dots\dots H_x, H_p(10), H_p(0.07)$$

$$D(TLw_1 + TLw_2, TLf_1 + TLf_2) = D(TLw_1, TLf_1) + D(TLw_2, TLf_2)$$

"if" dose algorithm 1:

$$\frac{TLf}{TLw} \geq 0.7 \Rightarrow K_a = N \cdot TLf$$

$\frac{TLf}{TLw} < 0.7 \Rightarrow$ "special" dose algorithm 2:

$$\Rightarrow \text{energy response } K_a = N \cdot \frac{TLw}{f_w \left(\frac{TLf}{TLw} \right)}$$

$f_w(R)$energy respons of TLw

\Rightarrow Energy response $\approx 0\%$



"linear" dose algorithm 3a:

$$H_p(10) = N \cdot (a \cdot TLw + (1 - a) \cdot TLf)$$

\Rightarrow Energy response $\approx \pm 15\%$

\Rightarrow Reference radiation quality

"linear" dose algorithm 3b:

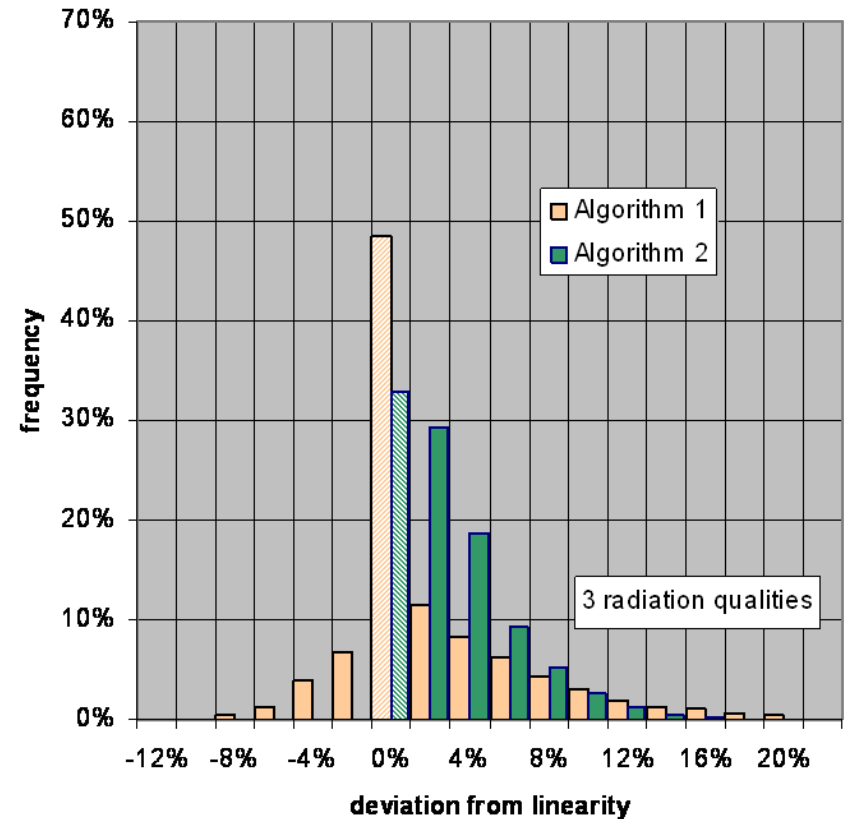
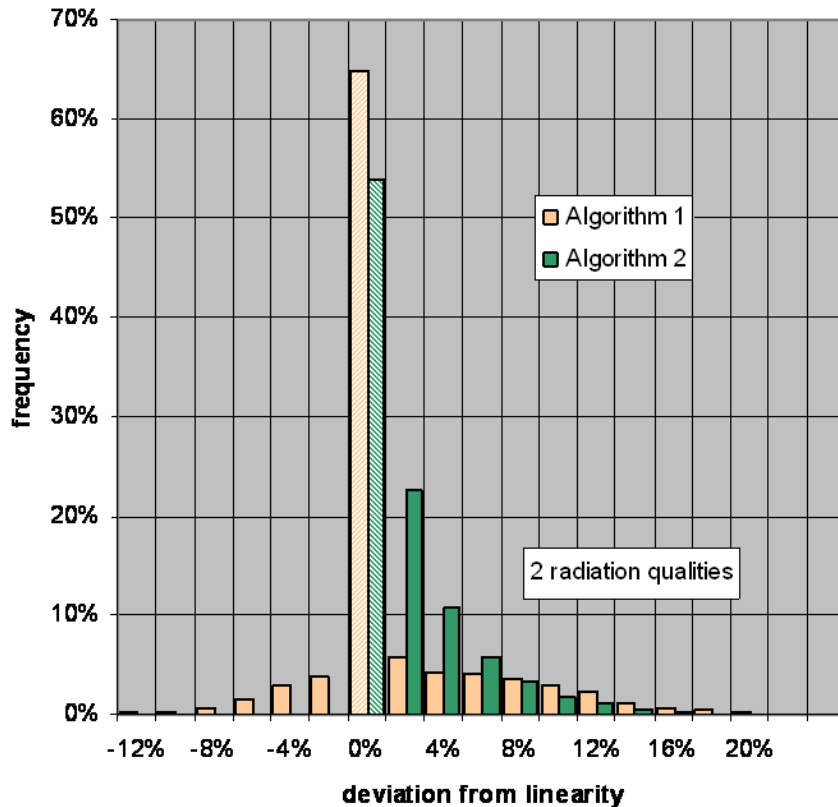
$$H_p(0.07) = N \cdot (b \cdot TLw + (1 - b) \cdot TLf)$$

\Rightarrow Energy response $< \pm 25\%$

\Rightarrow Reference radiation quality : N-120

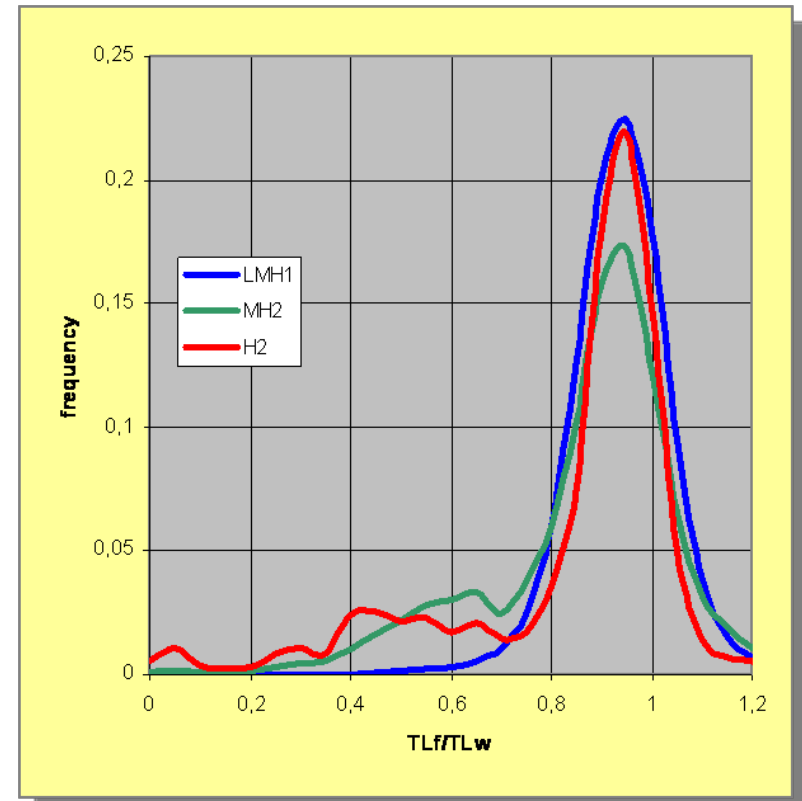
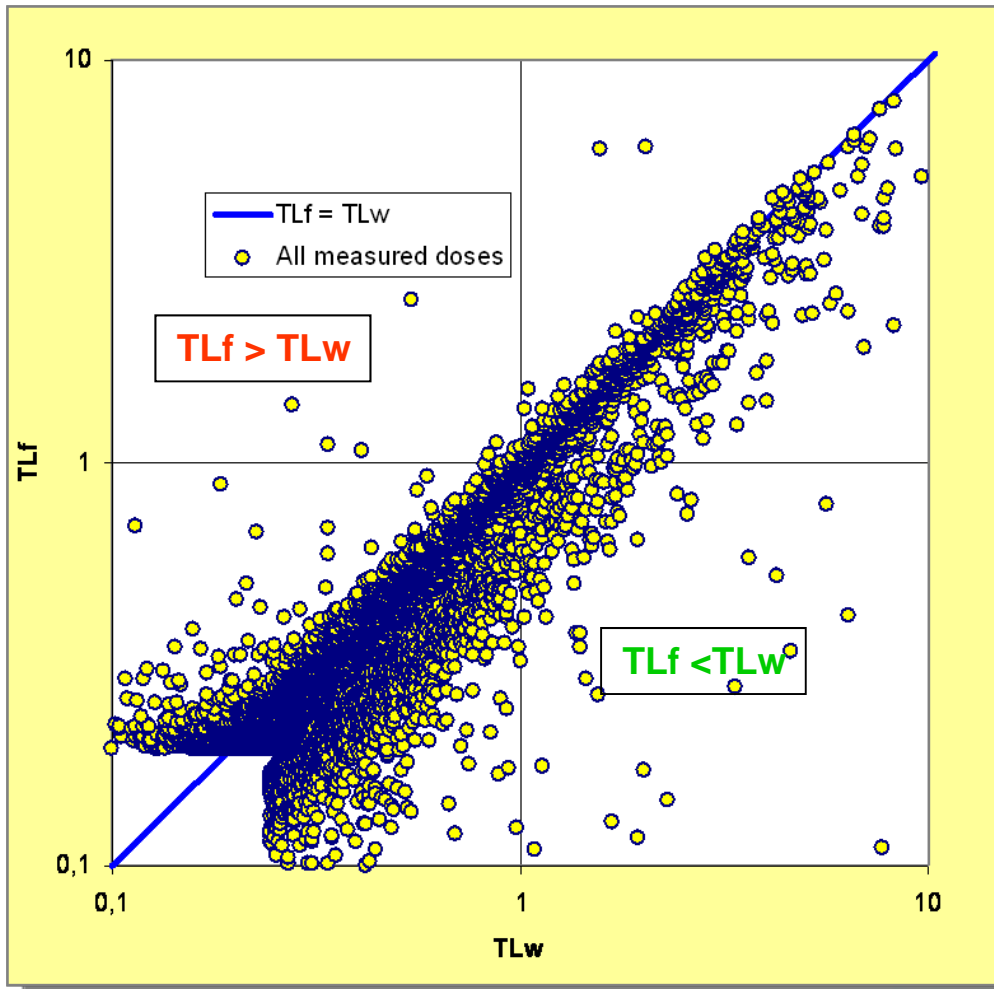


Simulation of „mixed fields“

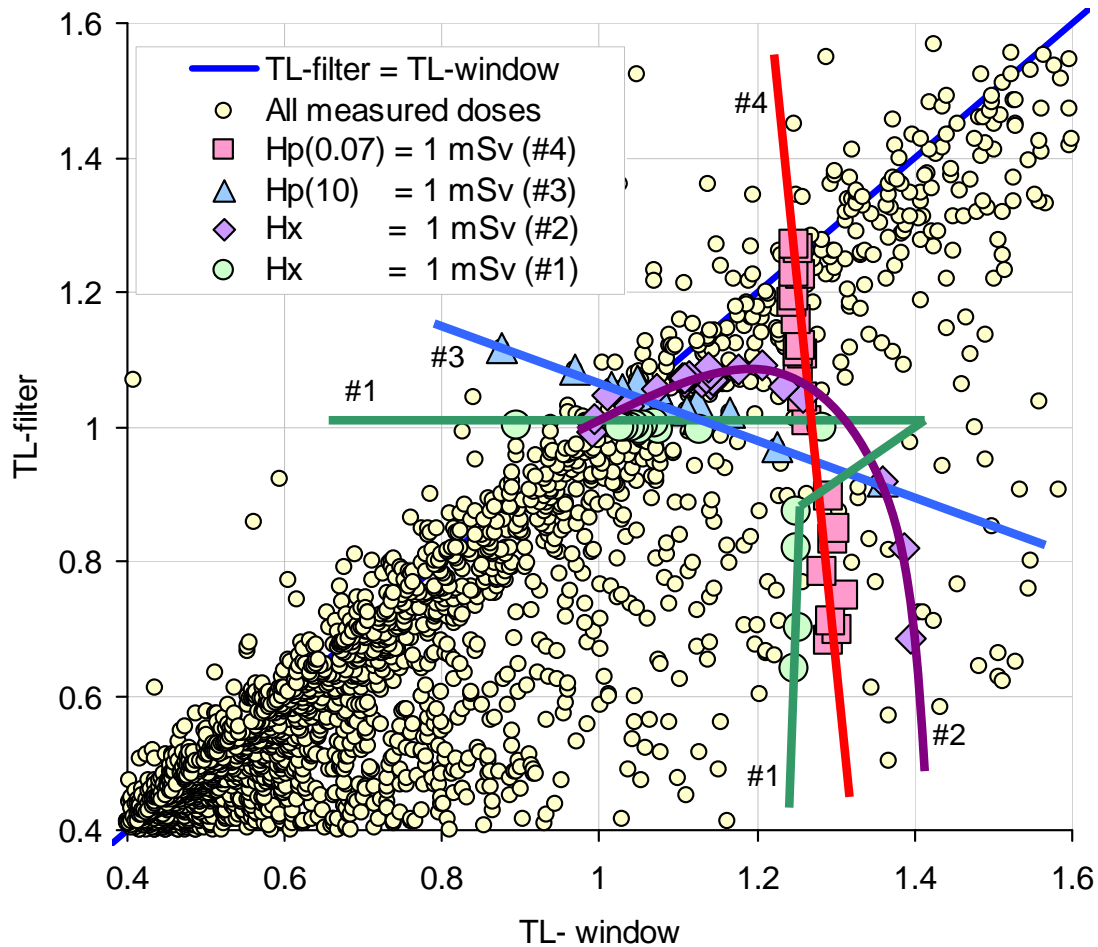


$$deviation = D(TLw_1 + TLw_2, TLf_1 + TLf_2) - (D(TLw_1, TLf_1) + D(TLw_2, TLf_2))$$

Single measured doses



Single measured doses



**The best directional
and energy response
does not work if ...**

